

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

APPLICATION FOR LETTERS PATENT

**Presentation Architecture for Network Supporting
Implantable Cardiac Therapy Devices**

Inventor(s):
Nirav Dalal

ATTORNEY'S DOCKET NO. SJ1-040US

10008592-110904

11/09/01



TECHNICAL FIELD

The present invention generally relates to implantable cardiac therapy devices and ways to present information obtained from the implantable therapy devices.

BACKGROUND

Implantable cardiac therapy devices (ICTDs) are implanted within the body of a patient to monitor, regulate, and/or correct heart function. ICTDs include implantable cardiac stimulation devices (e.g., implantable cardiac pacemakers, implantable defibrillators) that apply stimulation therapy to the heart as well as implantable cardiac monitors that monitor heart activity.

ICTDs typically include a control unit positioned within a casing that is implanted into the body and a set of leads that are positioned to impart stimulation and/or monitor cardiac activity. With improved processor and memory technologies, the control units have become increasingly more sophisticated, allowing them to monitor many types of conditions and apply tailored stimulation therapies in response to those conditions.

ICTDs are typically capable of being programmed remotely by an external programming device, often called a "programmer". Today, individual ICTDs are equipped with telemetry circuits that communicate with the programmer. One type of programmer utilizes an electromagnetic wand that is placed near the implanted cardiac device to communicate with the implanted device. When used in a sterile field, the wand may be enclosed in a sterile sheath. The wand contains a coil that forms a transformer coupling with the ICTD telemetry circuitry. The wand transmits low frequency signals by varying coil impedance.

1 Early telemetry systems were passive, meaning that the communication was
2 unidirectional from the programmer to the implanted device. Passive telemetry
3 allowed a treating physician to download instructions to the implanted device
4 following implantation. Due to power and size constraints, early commercial
5 versions of the implanted devices were incapable of transmitting information back
6 to the programmer.

7 As power capabilities improved, active telemetry became feasible, allowing
8 synchronous bi-directional communication between the implanted device and the
9 programmer. Active telemetry utilizes a half-duplex communication mode in
10 which the programmer sends instructions in a predefined frame format and,
11 following termination of this transmission, the implanted device returns data using
12 the frame format. With active telemetry, the treating physician is able to not only
13 program the implanted device, but also retrieve information from the implanted
14 device to evaluate heart activity and device performance. The treating physician
15 may periodically want to review device performance or heart activity data for
16 predefined periods of time to ensure that the device is providing therapy in desired
17 manner. Consequently, current generation implantable cardiac therapy devices
18 incorporate memories, and the processors periodically sample and record various
19 performance parameter measurements in the memories.

20 Data pertaining to a patient's cardiac condition is gathered and stored by
21 the programmer during programming sessions of the ICTDs. Analysis of the
22 cardiac condition is performed locally by the programming software.
23 Programmers offer comprehensive diagnostic capabilities, high-speed processing,
24 and easy operation, thereby facilitating efficient programming and timely patient
25 follow-up.

1 In addition to local analysis, TransTelephonic Monitoring (TTM) systems
2 are employed to gather current cardiac data from patients who are remote from the
3 healthcare provider. TTM systems are placed in patients' homes. They typically
4 include a base unit that gathers information from the ICTD much like the
5 programmer would. The base unit is connected to a telephone line so that data
6 may be transmitted to the medical staff responsible for that patient. An example of
7 an ICTD TTM system is a service from St. Jude Medical® and Raytel® Cardiac
8 Services called "Housecall™." This service provides current programmed
9 parameters and episode diagnostic information for a plurality of events including
10 stored electrograms (EGMs). Real-time EGMs with annotated status information
11 can also be transmitted.

12 Using a telephone and a transmitter, the TTM system provides both the
13 medical staff and the patient the convenience of instant analysis of therapy without
14 having the patient leave the comfort of home. Typically, real-time measurements
15 are transmitted in just minutes. Patients may be closely monitored, and the medical
16 staff has more control of their patient's treatment, thus administering better patient
17 management.

18 One challenge that still persists, however, is how to efficiently and
19 effectively present patient information and cardiac data to medical personnel and
20 other knowledge workers who might have an interest in the device data. People
21 utilize different types of computing devices to receive and view data, such as
22 computers, portable computers, personal digital assistants, facsimile machines, and
23 so on. These computing devices have different user interface capabilities and
24 features. Accordingly, there is a need for a system that delivers the data to a wide
25 variety of computing devices.

1
2 **SUMMARY**

3 A cardiac therapy network architecture collects data output by one or more
4 implantable cardiac therapy devices, processes that data, and distributes it to
5 various knowledge workers. The cardiac therapy network implements a
6 presentation architecture that formats and encodes the data using different formats
7 and protocols to facilitate distribution to and presentation on various computing
8 devices with different user interface capabilities.
9

10 **BRIEF DESCRIPTION OF THE DRAWINGS**

11 Fig. 1 is a diagrammatic illustration of a cardiac therapy network
12 architecture with an implantable cardiac therapy device (ICTD) connected to a
13 network of computing systems used by various knowledge workers.

14 Fig. 2 is a functional diagram illustrating information flow from the ICTD
15 to the computing systems associated with the knowledge workers.

16 Fig. 3 is a functional diagram illustrating how the various computing
17 systems share pieces of information to improve care given to the patient.

18 Fig. 4 is a functional diagram illustrating information flow from the
19 computing systems back to the ICTD.

20 Fig. 5 is a simplified illustration of an ICTD in electrical communication
21 with a patient's heart for monitoring heart activity and/or delivering stimulation
22 therapy.

23 Fig. 6 is a functional block diagram of an exemplary implantable cardiac
24 therapy device.
25

1 Fig. 7 is a functional block diagram of an exemplary computing device that
2 may be used in the computing systems of the cardiac therapy network architecture.

3 Fig. 8 illustrates a presentation architecture implemented by the network
4 architecture to facilitate distribution and presentation of information from the
5 ICTD to the knowledge workers.

6 Fig. 9 is a functional block diagram of an exemplary presentation system to
7 format and encode content for delivery to the knowledge workers.

8 Fig. 10 is a flow diagram of a method for presenting content to the
9 knowledge workers.

10 In the description that follows, like numerals or reference designators are
11 used to reference like parts or elements.

12 13 **DETAILED DESCRIPTION**

14 The following description sets forth a cardiac therapy network architecture in
15 which data collected from an implantable cardiac therapy device is processed and
16 distributed to various knowledge workers. It is anticipated that the knowledge
17 workers will utilize different computing devices for receiving and viewing the
18 data. These computing devices vary widely in terms of their user interface (UI)
19 capabilities. Accordingly, the network architecture implements a presentation
20 architecture that formats and distributes content to various computing devices with
21 different user interface capabilities.

22 23 **Cardiac Therapy Network**

24 Fig. 1 shows an exemplary cardiac therapy network architecture 100 that
25 includes an implantable cardiac therapy device (ICTD) 102 coupled to a network

1 of computing systems associated with various knowledge workers who have
2 interest in cardiac therapy. The ICTD is illustrated as being implanted in a human
3 patient 104. The ICTD 102 is in electrical communication with a patient's heart
4 106 by way of multiple leads 108 suitable for monitoring cardiac activity and/or
5 delivering multi-chamber stimulation and shock therapy.

6 The ICTD 102 may communicate with a standalone or offline programmer
7 110 via short-range telemetry technology. The offline programmer 110 is
8 equipped with a wand that, when positioned proximal to the ICTD 102,
9 communicates with the ICTD 102 through a magnetic coupling.

10 The ICTD 102 can alternatively, or additionally, communicate with a local
11 transceiver 112. The local transceiver 112 may be a device that resides on or near
12 the patient, such as an electronic communications device that is worn by the
13 patient or is situated on a structure within the room or residence of the patient.
14 The local transceiver 112 communicates with the ICTD 102 using short-range
15 telemetry or longer-range high-frequency-based telemetry, such as RF (radio
16 frequency) transmissions. Alternatively, the local transceiver 112 may be
17 incorporated into the ICTD 102, as represented by dashed line 111. In this case,
18 the ICTD includes a separate and isolated package area that accommodates high-
19 frequency transmissions without disrupting operation of the monitoring and
20 stimulation circuitry.

21 Depending upon the implementation and transmission range, the local
22 transceiver 112 can be in communication with various other devices of the
23 network architecture 100. One possible implementation is for the local transceiver
24 112 to transmit information received from the ICTD 102 to a networked
25 programmer 114, which is connected to network 120. The networked programmer

1 114 is similar in operation to standalone programmer 110, but differs in that it is
2 connected to the network 120. The networked programmer 114 may be local to, or
3 remote from, the local transceiver 112; or alternatively, the local transceiver 112
4 may be incorporated into the networked programmer 114, as represented by
5 dashed line 116.

6 Another possible implementation is for the local transceiver to be
7 connected directly to the network 120 for communication with remote computing
8 devices and/or programmers. Still another possibility is for the local transceiver
9 112 to communicate with the network 120 via wireless communication, such as
10 via a satellite system 122.

11 The network 120 may be implemented by one or more different types of
12 networks (e.g., Internet, local area network, wide area network, telephone, cable,
13 satellite, etc.), including wire-based technologies (e.g., telephone line, cable, fiber
14 optics, etc.) and/or wireless technologies (e.g., RF, cellular, microwave, IR,
15 wireless personal area network, etc.). The network 120 can be configured to
16 support any number of different protocols, including HTTP (HyperText Transport
17 Protocol), TCP/IP (Transmission Control Protocol/Internet Protocol), WAP
18 (Wireless Application Protocol), Bluetooth, and so on.

19 A number of knowledge workers are interested in data gathered from the
20 implantable cardiac therapy device 102. Representative knowledge workers
21 include healthcare providers 130, the device manufacturer 132, clinical groups
22 134, and regulatory agencies 136. The knowledge workers are interested in
23 different portions of the data. For instance, the healthcare providers 130 are
24 interested in information pertaining to a particular patient's condition. The
25 manufacturer 132 cares about how the device is operating. The clinical groups

1 134 want certain data for inclusion in patient populations that can be studied and
2 analyzed. The regulatory agencies 136 are concerned whether the devices, and
3 various treatments administered by them, are safe or pose a health risk.

4 The network architecture 100 facilitates distribution of the device data to
5 the various knowledge workers. Information gathered from the device is
6 integrated, processed, and distributed to the knowledge workers. Computer
7 systems maintain and store the device data, and prepare the data for efficient
8 presentation to the knowledge workers. The computer systems are represented
9 pictorially in Fig. 1 as databases. However, such system can be implemented
10 using a wide variety of computing devices, ranging from small handheld
11 computers or portable digital assistants (PDAs) carried by physicians to
12 workstations or mainframe computers with large storage capabilities. The
13 healthcare providers 130 are equipped with computer systems 140 that store and
14 process patient records 142. The manufacturer 132 has a computer system 144
15 that tracks device data 146 returned from ICTDs 102. The clinical groups 134
16 have computer systems 148 that store and analyze data across patient populations,
17 as represented by a histogram 150. The regulatory agencies 136 maintain
18 computer systems 152 that register and track healthcare risk data 154 for ICTDs.

19 The network architecture 100 supports two-way communication. Not only
20 is data collected from the ICTD 102 and distributed to the various computer
21 systems of the knowledge workers, but also information can be returned from
22 these computer systems to the networked programmer 114 and/or the local
23 transceiver 112 for communication back to the ICTD 102. Information returned to
24 the ICTD 102 may be used to adjust operation of the device, or modify therapies
25

1 being applied by the device. Such information may be imparted to the ICTD 102
2 automatically, without the patient's knowledge.

3 Additionally, information may be sent to a patient notification device 160 to
4 notify the patient of some event or item. The patient notification device 160 can
5 be implemented in a number of ways including, for example, as a telephone, a
6 cellular phone, a pager, a PDA (personal digital assistant), a dedicated patient
7 communication device, a computer, an alarm, and so on. Notifications may be as
8 simple as an instruction to sound an alarm to inform the patient to call into the
9 healthcare providers, or as complex as HTML-based pages with graphics and
10 textual data to educate the patient. Notification messages sent to the patient
11 notification device 160 can contain essentially any type of information related to
12 cardiac medicinal purposes or device operation. Such information might include
13 new studies released by clinical groups pertaining to device operation and patient
14 activity (e.g., habits, diets, exercise, etc.), recall notices or operational data from
15 the manufacturer, patient-specific instructions sent by the healthcare providers, or
16 warnings published by regulatory groups.

17 Notifications can be sent directly from the knowledge worker to the patient.
18 Additionally, the network architecture 100 may include a notification system 170
19 that operates computer systems 172 designed to create and deliver notification
20 messages 174 on behalf of the knowledge workers. The notification system 170
21 delivers the messages in formats supported by the various types of patient
22 notification devices 160. For instance, if the patient carries a pager, a notification
23 message might consist of a simple text statement in a pager protocol. For a more
24 sophisticated wireless-enabled PDA or Internet-oriented cellular phone, messages
25 might contain more than text data and be formatted using WAP formats.

Fig. 2 shows the flow of data from the implantable cardiac therapy device 102 to the various computer systems used by the knowledge workers. Data from the ICTD is output as digital data, as represented by the string of 0's and 1's. The data may consist of any number of items, including heart activity (e.g., IEGM), patient information, device operation, analysis results from on-device diagnostics, and so on.

A data integrator 200 accumulates the data and stores it in a repository 202. A processing system 204 processes portions of the data according to various applications 206 that are specifically tailored to place the data into condition for various knowledge workers. For example, healthcare workers might be interested in certain portions of the data, such as the IEGM data and the patient information. Clinical scientists might be interested in the heart data, but do not wish to see any patient information. Manufacturers may be interested in the raw data stream itself as a tool to discern how the device is operating. Depending on the needs of the end worker, the processing system 204 takes the raw device data, evaluates its accuracy and completeness, and generates different packages of data for delivery to the various knowledge workers. The processed data packages are also stored in the repository 202.

When the data is ready for delivery, a distribution/presentation system 208 distributes the different packages to the appropriate computer systems 140, 144, 148, 152, and 172. The distribution/presentation system 208 is configured to serve the packages according to the protocols and formats desired by the computer systems. In this manner, the network architecture 100 allows relevant portions of device data, collected from the ICTD, to be disseminated to the appropriate knowledge workers in a form they prefer.

1 Once the ICTD data is delivered, the computer systems 140, 144, 148, 152,
2 and 172 store the data and/or present the data to the knowledge worker. The
3 computer systems may perform further processing specific to their use of the data.
4 Through these processes, the knowledge workers create additional information
5 that is useful to the patient, or other knowledge workers with interests in ICTDs.
6 For example, from the ICTD data, the knowledge workers might devise improved
7 therapies for a given patient, or create instructions to modify operation of a
8 specific ICTD, or gain a better understanding of how implantable cardiac devices
9 operate in general, or develop better technologies for future generations of ICTDs.
10 Much of this created knowledge can be shared among the various knowledge
11 workers.

12 Fig. 3 shows how the various computing systems 140, 144, 148, 152, and
13 172 can cooperate and share pieces of information to improve the care given to a
14 patient. Where appropriate and legally acceptable, the computer systems may be
15 configured to pass non-private information among the various knowledge workers
16 to better improve their understanding of the implantable medical field. Clinical
17 results 150 produced by the clinical computer systems 148 may be shared with
18 healthcare providers to improve patient care or with manufacturers to help in their
19 design of next generation devices. The sharing of information may further lead to
20 better and timelier healthcare for the patients.

21 If the collective knowledge base produces information that may prove
22 helpful to the patient, that information can be passed to the notification system 172
23 for delivery to one or more patients. Also, any one of the knowledge workers may
24 wish to employ the notification system 172 to send messages to the patient(s).
25

Fig. 4 shows, in more detail, the flow of information back from the various computer systems used by the knowledge workers to the implantable cardiac therapy device 102 or the patient notification device 160. Information from any one of the computing systems—healthcare computer system(s) 140, manufacturer computer system(s) 144, clinical computer system(s) 148, regulatory computer system(s) 152—or the notification system 172 can be sent to a patient feedback system 400. The patient feedback system 400 facilitates delivery of the information back to the patient. It may be an independent system, or incorporated into one or more of the computing. It may alternatively be integrated into the notification system 172.

The patient feedback system 400 may be implemented in many ways. As one exemplary implementation, the patient feedback system 400 is implemented as a server that serves content back to the networked programmer 114, which then uses the information to program the ICTD 102 through a built in transceiver 116, local transceiver 112, or wand-based telemetry. As another possible implementation, the patient feedback system may be a cellular or RF transmission system that sends information back to the patient feedback device 160.

The network architecture 100 facilitates continuous care around the clock, regardless of where the patient is located. For instance, suppose the patient is driving in the car when a cardiac episode occurs. The ICTD 102 detects the condition and transmits an alert message about the condition to the local transceiver 112. The message is processed and delivered to a physician's computer or PDA via the network 120. The physician can make a diagnosis and send some instructions back to the patient's ICTD. The physician might also have a notification message that guides the patient to a nearest healthcare facility for

1 further treatment sent via the notification system 170 to the patient's notification
2 device 160. Concurrently, the physician can share the patient's records online with
3 an attending physician at the healthcare facility so that the attending physician can
4 review the records prior to the patient's arrival.

6 Exemplary ICTD

7 Fig. 5 shows an exemplary ICTD 102 in electrical communication with a
8 patient's heart 106 for monitoring heart activity and/or delivering stimulation
9 therapy, such as pacing or defibrillation therapies. The ICTD 102 is in electrical
10 communication with a patient's heart 106 by way of three leads 108(1)-(3). To
11 sense atrial cardiac signals and to provide right atrial chamber stimulation therapy,
12 the ICTD 102 is coupled to an implantable right atrial lead 108(1) having at least
13 an atrial tip electrode 502, which typically is implanted in the patient's right atrial
14 appendage. To sense left atrial and ventricular cardiac signals and to provide left
15 chamber pacing therapy, the ICTD 102 is coupled to a coronary sinus lead 108(2)
16 designed for placement in the coronary sinus region via the coronary sinus. The
17 coronary sinus lead 108(2) positions a distal electrode adjacent to the left ventricle
18 and/or additional electrode(s) adjacent to the left atrium. An exemplary coronary
19 sinus lead 108(2) is designed to receive atrial and ventricular cardiac signals and
20 to deliver left ventricular pacing therapy using at least a left ventricular tip
21 electrode 504, left atrial pacing therapy using at least a left atrial ring electrode
22 506, and shocking therapy using at least a left atrial coil electrode 508.

23 The ICTD 102 is also shown in electrical communication with the patient's
24 heart 106 by way of an implantable right ventricular lead 108(3) having, in this
25 implementation, a right ventricular tip electrode 510, a right ventricular ring

1 electrode 512, a right ventricular (RV) coil electrode 514, and an SVC coil
2 electrode 516. Typically, the right ventricular lead 108(3) is transvenously
3 inserted into the heart 102 to place the right ventricular tip electrode 510 in the
4 right ventricular apex so that the RV coil electrode 514 will be positioned in the
5 right ventricle and the SVC coil electrode 516 will be positioned in the superior
6 vena cava. Accordingly, the right ventricular lead 108(3) is capable of receiving
7 cardiac signals, and delivering stimulation in the form of pacing and shock therapy
8 to the right ventricle.

9 Fig. 6 shows an exemplary, simplified block diagram depicting various
10 components of the ICTD 102. The ICTD 102 can be configured to perform one or
11 more of a variety of functions including, for example, monitoring heart activity,
12 monitoring patient activity, and treating fast and slow arrhythmias with stimulation
13 therapy that includes cardioversion, defibrillation, and pacing stimulation. While a
14 particular multi-chamber device is shown, it is to be appreciated and understood
15 that this is done for illustration purposes.

16 The circuitry is housed in housing 600, which is often referred to as the
17 "can", "case", "encasing", or "case electrode", and may be programmably selected
18 to act as the return electrode for unipolar modes. Housing 600 may further be
19 used as a return electrode alone or in combination with one or more of the coil
20 electrodes for shocking purposes. Housing 600 further includes a connector (not
21 shown) having a plurality of terminals 602, 604, 606, 608, 612, 614, 616, and 618
22 (shown schematically and, for convenience, the names of the electrodes to which
23 they are connected are shown next to the terminals).

24 To achieve right atrial sensing and pacing, the connector includes at least a
25 right atrial tip terminal (A_R TIP) 602 adapted for connection to the atrial tip

electrode 502. To achieve left chamber sensing, pacing, and shocking, the connector includes at least a left ventricular tip terminal (V_L TIP) 604, a left atrial ring terminal (A_L RING) 606, and a left atrial shocking terminal (A_L COIL) 608, which are adapted for connection to the left ventricular ring electrode 504, the left atrial ring electrode 506, and the left atrial coil electrode 508, respectively. To support right chamber sensing, pacing, and shocking, the connector includes a right ventricular tip terminal (V_R TIP) 612, a right ventricular ring terminal (V_R RING) 614, a right ventricular shocking terminal (RV COIL) 616, and an SVC shocking terminal (SVC COIL) 618, which are adapted for connection to the right ventricular tip electrode 510, right ventricular ring electrode 512, the RV coil electrode 514, and the SVC coil electrode 516, respectively.

At the core of the ICTD 102 is a programmable microcontroller 620 that controls various operations of the ICTD, including cardiac monitoring and stimulation therapy. Microcontroller 620 includes a microprocessor (or equivalent control circuitry), RAM and/or ROM memory, logic and timing circuitry, state machine circuitry, and I/O circuitry. Microcontroller 620 includes the ability to process or monitor input signals (data) as controlled by a program code stored in a designated block of memory. Any suitable microcontroller 620 may be used. The use of microprocessor-based control circuits for performing timing and data analysis functions are well known in the art.

For discussion purposes, microcontroller 620 is illustrated as including timing control circuitry 632 to control the timing of the stimulation pulses (e.g., pacing rate, atrio-ventricular (AV) delay, atrial interconduction (A-A) delay, or ventricular interconduction (V-V) delay, etc.) as well as to keep track of the timing of refractory periods, blanking intervals, noise detection windows, evoked

1 response windows, alert intervals, marker channel timing, and so on.
2 Microcontroller 220 may further include various types of cardiac condition
3 detectors 634 (e.g., an arrhythmia detector, a morphology detector, etc.) and
4 various types of compensators 636 (e.g., orthostatic compensator, syncope
5 response module, etc.). These components can be utilized by the device 102 for
6 determining desirable times to administer various therapies. The components 632-
7 636 may be implemented in hardware as part of the microcontroller 620, or as
8 software/firmware instructions programmed into the device and executed on the
9 microcontroller 620 during certain modes of operation.

10 The ICTD 102 further includes an atrial pulse generator 622 and a
11 ventricular pulse generator 624 that generate pacing stimulation pulses for delivery
12 by the right atrial lead 108(1), the coronary sinus lead 108(2), and/or the right
13 ventricular lead 108(3) via an electrode configuration switch 626. It is understood
14 that in order to provide stimulation therapy in each of the four chambers of the
15 heart, the atrial and ventricular pulse generators, 622 and 624, may include
16 dedicated, independent pulse generators, multiplexed pulse generators, or shared
17 pulse generators. The pulse generators 622 and 624 are controlled by the
18 microcontroller 620 via appropriate control signals 628 and 630, respectively, to
19 trigger or inhibit the stimulation pulses.

20 The electronic configuration switch 626 includes a plurality of switches for
21 connecting the desired electrodes to the appropriate I/O circuits, thereby providing
22 complete electrode programmability. Accordingly, switch 626, in response to a
23 control signal 642 from the microcontroller 620, determines the polarity of the
24 stimulation pulses (e.g., unipolar, bipolar, combipolar, etc.) by selectively closing
25 the appropriate combination of switches (not shown).

1 Atrial sensing circuits 644 and ventricular sensing circuits 646 may also be
2 selectively coupled to the right atrial lead 108(1), coronary sinus lead 108(2), and
3 the right ventricular lead 108(3), through the switch 626 to detect the presence of
4 cardiac activity in each of the four chambers of the heart. Accordingly, the atrial
5 (ATR. SENSE) and ventricular (VTR. SENSE) sensing circuits, 644 and 646, may
6 include dedicated sense amplifiers, multiplexed amplifiers, or shared amplifiers.
7 Each sensing circuit 644 and 646 may further employ one or more low power,
8 precision amplifiers with programmable gain and/or automatic gain control,
9 bandpass filtering, and a threshold detection circuit to selectively sense the cardiac
10 signal of interest. The automatic gain control enables the ICTD 102 to deal
11 effectively with the difficult problem of sensing the low amplitude signal
12 characteristics of atrial or ventricular fibrillation. Switch 626 determines the
13 "sensing polarity" of the cardiac signal by selectively closing the appropriate
14 switches. In this way, the clinician may program the sensing polarity independent
15 of the stimulation polarity.

16 The outputs of the atrial and ventricular sensing circuits 644 and 646 are
17 connected to the microcontroller 620 which, in turn, is able to trigger or inhibit the
18 atrial and ventricular pulse generators 622 and 624, respectively, in a demand
19 fashion in response to the absence or presence of cardiac activity in the
20 appropriate chambers of the heart. The sensing circuits 644 and 646 receive
21 control signals over signal lines 648 and 650 from the microcontroller 620 for
22 purposes of controlling the gain, threshold, polarization charge removal circuitry
23 (not shown), and the timing of any blocking circuitry (not shown) coupled to the
24 inputs of the sensing circuits 644 and 646.
25

1 Cardiac signals are also applied to inputs of an analog-to-digital (A/D) data
2 acquisition system 652. The data acquisition system 652 is configured to acquire
3 intracardiac electrogram signals, convert the raw analog data into a digital signal,
4 and store the digital signals for later processing and/or telemetric transmission to
5 an external device 654. The data acquisition system 652 is coupled to the right
6 atrial lead 108(1), the coronary sinus lead 108(2), and the right ventricular lead
7 108(3) through the switch 626 to sample cardiac signals across any pair of desired
8 electrodes.

9 The data acquisition system 652 may be coupled to the microcontroller 620,
10 or other detection circuitry, to detect an evoked response from the heart 106 in
11 response to an applied stimulus, thereby aiding in the detection of "capture".
12 Capture occurs when an electrical stimulus applied to the heart is of sufficient
13 energy to depolarize the cardiac tissue, thereby causing the heart muscle to
14 contract. The microcontroller 620 detects a depolarization signal during a window
15 following a stimulation pulse, the presence of which indicates that capture has
16 occurred. The microcontroller 620 enables capture detection by triggering the
17 ventricular pulse generator 624 to generate a stimulation pulse, starting a capture
18 detection window using the timing control circuitry 632 within the microcontroller
19 620, and enabling the data acquisition system 652 via control signal 656 to sample
20 the cardiac signal that falls in the capture detection window and, based on the
21 amplitude, determines if capture has occurred.

22 The microcontroller 620 is further coupled to a memory 660 by a suitable
23 data/address bus 662, wherein the programmable operating parameters used by the
24 microcontroller 620 are stored and modified, as required, in order to customize the
25 operation of the implantable device 102 to suit the needs of a particular patient.

1 physiologic sensors that may be implemented in device 102 include known
2 sensors that, for example, sense respiration rate and/or minute ventilation, pH of
3 blood, ventricular gradient, and so forth.

4 The ICTD 102 additionally includes a battery 676 that provides operating
5 power to all of circuits shown in Fig. 2. If the device 102 is configured to deliver
6 pacing or shocking therapy, the battery 676 is capable of operating at low current
7 drains for long periods of time (e.g., preferably less than 10 μ A), and is capable of
8 providing high-current pulses (for capacitor charging) when the patient requires a
9 shock pulse (e.g., preferably, in excess of 2 A, at voltages above 2 V, for periods of
10 10 seconds or more). The battery 676 also desirably has a predictable discharge
11 characteristic so that elective replacement time can be detected. As one example,
12 the device 102 employs lithium/silver vanadium oxide batteries.

13 The ICTD 102 can further include magnet detection circuitry (not shown),
14 coupled to the microcontroller 620, to detect when a magnet is placed over the
15 device 102. A magnet may be used by a clinician to perform various test functions
16 of the device 102 and/or to signal the microcontroller 620 that the external
17 programmer is in place to receive or transmit data to the microcontroller 620
18 through the telemetry circuits 664.

19 The ICTD 102 further includes an impedance measuring circuit 678 that is
20 enabled by the microcontroller 620 via a control signal 680. Uses for an
21 impedance measuring circuit 678 include, but are not limited to, lead impedance
22 surveillance during the acute and chronic phases for proper lead positioning or
23 dislodgement; detecting operable electrodes and automatically switching to an
24 operable pair if dislodgement occurs; measuring respiration or minute ventilation;
25 measuring thoracic impedance for determining shock thresholds; detecting when

1 the device has been implanted; measuring stroke volume; and detecting the
2 opening of heart valves, etc. The impedance measuring circuit 678 is
3 advantageously coupled to the switch 626 so that any desired electrode may be
4 used.

5 In the case where the device 102 is intended to operate as an implantable
6 cardioverter/defibrillator (ICD) device, it detects the occurrence of an arrhythmia,
7 and automatically applies an appropriate electrical shock therapy to the heart
8 aimed at terminating the detected arrhythmia. To this end, the microcontroller 620
9 further controls a shocking circuit 682 by way of a control signal 684. The
10 shocking circuit 682 generates shocking pulses of low (up to 0.5 Joules), moderate
11 (0.5 - 10 Joules), or high energy (11 to 40 Joules), as controlled by the
12 microcontroller 620. Such shocking pulses are applied to the patient's heart 106
13 through at least two shocking electrodes, and as shown in this implementation,
14 selected from the left atrial coil electrode 508, the RV coil electrode 514, and/or
15 the SVC coil electrode 516. As noted above, the housing 600 may act as an active
16 electrode in combination with the RV coil electrode 514, or as part of a split
17 electrical vector using the SVC coil electrode 516 or the left atrial coil electrode
18 508 (i.e., using the RV electrode as a common electrode).

19 Cardioversion shocks are generally considered to be of low to moderate
20 energy level (so as to minimize pain felt by the patient), and/or synchronized with
21 an R-wave and/or pertaining to the treatment of tachycardia. Defibrillation shocks
22 are generally of moderate to high energy level (i.e., corresponding to thresholds in
23 the range of 5-40 Joules), delivered asynchronously (since R-waves may be too
24 disorganized), and pertaining exclusively to the treatment of fibrillation.

1 Accordingly, the microcontroller 620 is capable of controlling the synchronous or
2 asynchronous delivery of the shocking pulses.

3 The ICTD 102 may further be designed with the ability to support high-
4 frequency wireless communication, typically in the radio frequency (RF) range.
5 As illustrated in Fig. 2, the can 600 may be configured with a secondary, isolated
6 casing 690 that contains circuitry for handling high-frequency signals. Within this
7 separate case 690 are a high-frequency transceiver 692 and a diplexer 694. High-
8 frequency signals received by a dedicated antenna, or via leads 108, are passed to
9 the transceiver 692. Due to the separate casing region 690, the transceiver handles
10 the high-frequency signals in isolation apart from the cardiac therapy circuitry. In
11 this manner, the high-frequency signals can be safely handled, thereby improving
12 telemetry communication, without adversely disrupting operation of the other
13 device circuitry.

14 Exemplary Computing Device

15 Fig. 7 shows an exemplary computing device 700 employed in the
16 computing systems of the cardiac therapy network architecture 100. It includes a
17 processing unit 702 and memory 704. Memory 704 includes both volatile
18 memory 706 (e.g., RAM) and non-volatile memory 708 (e.g., ROM, EEPROM,
19 Flash, disk, optical discs, persistent storage, etc.). An operating system and
20 various application programs 710 are stored in non-volatile memory 708. When a
21 program is running, various instructions are loaded into volatile memory 706 and
22 executed by processing unit 702. Examples of possible applications that may be
23 stored and executed on the computing device include the knowledge worker
24 specific applications 206 shown in Fig. 2.
25

1 The computing device 700 may further be equipped with a network I/O
2 connection 720 to facilitate communication with a network. The network I/O 720
3 may be a wire-based connection (e.g., network card, modem, etc.) or a wireless
4 connection (e.g., RF transceiver, Bluetooth device, etc.). The computing device
5 700 may also include a user input device 722 (e.g., keyboard, mouse, stylus, touch
6 pad, touch screen, voice recognition system, etc.) and an output device 724 (e.g.,
7 monitor, LCD, speaker, printer, etc.).

8 Various aspects of the methods and systems described throughout this
9 disclosure may be implemented in computer software or firmware as computer-
10 executable instructions. When executed, these instructions direct the computing
11 device (alone, or in concert with other computing devices of the system) to
12 perform various functions and tasks that enable the cardiac therapy network
13 architecture 100.

14 **Presentation Architecture**

15 One feature of the network architecture is a presentation architecture that
16 enables presentation of data obtained from the implantable cardiac therapy device
17 to various knowledge workers. The presentation architecture places the data in a
18 suitable format and protocol to accommodate different types of computing devices
19 with different UI capabilities. The presentation architecture separates the
20 processing and presentation functions so that decisions regarding how to present
21 the content are made independently of the collection and processing of the data.

22 Fig. 8 shows the presentation architecture 800 that is implemented by the
23 network architecture. The presentation architecture 800 has three layers: an
24 information source layer 802, a processing layer 804, and a presentation layer 806.
25

The information source layer 802 provides the data or information that is to be processed and presented to the knowledge worker. This layer includes data output by the ICTD, such as heart activity (e.g., IEGM), patient information, device operation data, analysis results from on-device diagnostics, and so on. It may further include other information made available for purposes of processing or better understanding the ICTD data.

The processing layer 804 performs the data handling and analytical processes. This layer contains the applications and methods that conform the data into content that will ultimately be presented to the knowledge workers. The processing layer 804 may include, for example, the processing system 204 and applications 206 that create the content desired by the knowledge workers.

The presentation layer 806 is responsible for getting the content to the knowledge worker in a form they prefer. This layer 806 contains the applications and processes that determine which content to present to whom, the format of the content, and the protocol by which to send the content.

Fig. 9 shows one exemplary implementation of the presentation layer 806 configured as the distribution/presentation system 208. The presentation layer 806 enables effective delivery and presentation of content to many different types of computing devices, as represented by exemplary devices 900(1)-(8). It is anticipated that knowledge workers will utilize many diverse types of computing devices, including pagers 900(1), personal digital assistants (PDAs) 900(2), Web-enabled or "smart" phones 900(3), portable computers 900(4), facsimile machines 900(5), cellular phones 900(6), databases 900(7), and desktop computers 900(8). These devices may be implemented using open standard software and protocols, or proprietary software and protocols.

1 knowledge worker. There are many possible protocols, including HTTP, TCP/IP,
2 WAP, Bluetooth, etc. Depending upon the preferences specified in the knowledge
3 worker records 906, the delivery protocol encoder 922 encodes the content to the
4 appropriate delivery protocol for subsequent distribution to the devices operated
5 by the knowledge workers.

6 Separating the presentation and processing layers and implementing UI
7 definitions and style sheets enables the architecture to distribute content produced
8 by multiple applications to a wide assortment of computing devices without
9 requiring unique UIs for each computing device. Suppose there are three
10 applications that produce content to be distributed to four different computing
11 devices of the knowledge workers. If the presentation layer were integrated with
12 the processing layer, the application developer would need to write a specific UI
13 for each device, resulting in twelve different versions of UI code (i.e., the number
14 of applications times the number of devices).

15 By separating the presentation layer, however, independent UI definitions
16 912(1)-(3) can be developed to specify UI requirements imposed by individual
17 applications. Style sheets 910(1)-(4) can be created to describe what features
18 individual devices are able to support. Combining the UI definition with a style
19 sheet dictates what content is presented and how it is presented for a given
20 computing device. In this example, the architecture allows, at most, the creation
21 of seven definitions/sheets to facilitate presentation of content from three
22 applications on four devices (i.e., the number of applications plus the number of
23 devices), down from twelve separate versions.

24 This architecture is easily adopted to support new computing devices. A
25 developer defines a new UI definition and/or a style sheet to enable presentation of

1 content on the new device. This saves time and money in that developers are not
2 forced to modify applications as UI capabilities of the end-user computing devices
3 change.

4 5 **Presentation Operation**

6 Fig. 10 shows a process 1000 for presenting content to the knowledge
7 workers. Aspects of this process may be implemented in hardware, firmware, or
8 software, or a combination thereof.

9 At block 1002, the distribution/presentation system 208 determines what
10 computing resources are available for the knowledge worker who is intended to
11 receive the information. The system consults the knowledge worker records 906
12 to identify the types of computing devices specified by the knowledge worker. At
13 block 1004, the system ascertains the features and capabilities of the computing
14 resources of the intended knowledge worker. Such features may include display
15 type, display size, graphical capabilities, color capabilities, etc.

16 At block 1006, the content selector 904 selects the content to be delivered
17 to the knowledge worker based, in part, on the capabilities of the computing
18 resources. For instance, if the knowledge worker is carrying a PDA or phone of
19 limited screen size, the content selector 904 extracts summary statements or
20 phrases from the content component store 902 that can be presented on the device.
21 For instance, the content selector might choose a statement "IEGM for Patient X is
22 ready for viewing". Such a message would inform the knowledge worker that
23 pertinent patient data is ready for downloading next time the knowledge worker is
24 at a device capable of viewing and analyzing IEGM charts. For devices of higher
25

capabilities (e.g., portable or desktop computer), the content selector may choose full data graphs and/or commentary to present to the knowledge worker.

At block 1008, the content formatter 920 formats the selected content into suitable formats for presentation on the knowledge worker's computing device. Possible formats include HTML, XML, and SNMP. At block 1010, the delivery protocol encoder 922 encodes the content according to a protocol supported by the target network and computing device. Examples of possible protocols include HTTP, TCP/IP, WAP, Bluetooth, etc. At block 1012, the system 208 delivers the content to the knowledge worker's computing device, where it is presented for review and analysis by the knowledge worker.

Conclusion

Although the invention has been described in language specific to structural features and/or methodological acts, it is to be understood that the subject matter defined in the appended claims is not necessarily limited to the specific features or acts described. Rather, the specific features and acts are disclosed as exemplary forms of implementing the claimed invention.